Power and shift independent imaging of coherent sources

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2 Algorithm

3 Simulations



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Measuring brain activity

ECoG

invasive

fMRI bad temporal resolution (\approx 1s)

MEG

EEG









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Two problems: signal leakage and ill-posedness



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- 1 Compute inverse (ROI, atlas or sparce grid)
- 2 Select seeds or go all-to-all
- **3** Use measures insensitive to signal leakage, e.g:
 - ImCoh [Nolte et al., 2004]
 - PLI
 - wPLI
 - Geometric correction scheme [Wens et al., Human Brain Mapping, 2015]

- 1 Compute inverse (ROI, atlas or sparce grid)
- 2 Select seeds or go all-to-all
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Problems of this approach

- 1 SL-proof connectivity measures lead to SNR loss
- 2 Inverse solution is affected by signal leakage

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Generative model

$$\begin{pmatrix} m_1 \\ m_2 \end{pmatrix} (t) = \begin{pmatrix} g_1^1 & g_2^1 \\ g_1^2 & g_2^1 \end{pmatrix} \begin{pmatrix} s_1 \\ s_2 \end{pmatrix} (t) = \\ = \begin{pmatrix} g_1^1 \\ g_1^2 \end{pmatrix} s_1(t) + \begin{pmatrix} g_2^1 \\ g_2^2 \end{pmatrix} s_2(t) = \vec{g}_1 s_1(t) + \vec{g}_2 s_2(t)$$
(1)

 $m_{1,2}(t)$ - MEG/EEG measurements $\{g_i^j\}$ - matrix of a forward model $s_{1,2}(t)$ - unknown timeseries on cortex

Time-frequency transformation

Apply time-frequency transform to (1)...

$$\begin{pmatrix} M_1 \\ M_2 \end{pmatrix} (f,t) = \vec{g}_1 S_1(f,t) + \vec{g}_2 S_2(f,t)$$
(2)

... and write cross-spectrum:

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$$\mathbf{C}^{MM}(t,f) \stackrel{def}{=} \mathbf{E}\{\mathbf{M}(t,f)\mathbf{M}^{H}(t,f)\}$$
(3)

N.B.

 M_1, M_2, S_1, S_2 after time-frequency transformation are complex

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Let's substitute (2) into (3)

$$\mathbf{C}^{MM}(t,f) = \mathbf{E} \left\{ \begin{pmatrix} M_1 \bar{M}_1 & M_1 \bar{M}_2 \\ M_2 \bar{M}_1 & M_2 \bar{M}_2 \end{pmatrix} (f,t) \right\} = \\ \mathbf{E} \left\{ \left(\vec{g}_1 S_1(f,t) + \vec{g}_2 S_2(f,t) \right) \cdot \left(\vec{g}_1^T \bar{S}_1(f,t) + \vec{g}_2^T \bar{S}_2(f,t) \right) \right\}$$
(4)

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$$\mathbf{C}^{MM}(t,f) = \mathbf{E} \left\{ \begin{pmatrix} M_1 \bar{M}_1 & M_1 \bar{M}_2 \\ M_2 \bar{M}_1 & M_2 \bar{M}_2 \end{pmatrix} (f,t) \right\} = \\ \mathbf{E} \left\{ \begin{pmatrix} \bar{g}_1 S_1(f,t) + \bar{g}_2 S_2(f,t) \end{pmatrix} \cdot \begin{pmatrix} \bar{g}_1^T \bar{S}_1(f,t) + \bar{g}_2^T \bar{S}_2(f,t) \end{pmatrix} \right\}$$
(4)

N.B. $\vec{g_i}$ are real $\implies \vec{g_i}^H = \vec{g_i}^T$

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Let's substitute (2) into (3)

$$\mathbf{C}^{MM}(t,f) = = \vec{g_1} \vec{g_1}^T \mathbf{E} \{ S_1(f,t) \bar{S_1}(f,t) \} + \vec{g_1} \vec{g_2}^T \mathbf{E} \{ S_1(f,t) \bar{S_2}(f,t) \} + + \vec{g_2} \vec{g_1}^T \mathbf{E} \{ S_2(f,t) \bar{S_1}(f,t) \} + \vec{g_2} \vec{g_2}^T \mathbf{E} \{ S_2(f,t) \bar{S_2}(f,t) \}$$
(4)

Finally, we've got

$$\begin{pmatrix} c_{11}^{MM} & c_{12}^{MM} \\ c_{21}^{MM} & c_{22}^{MM} \end{pmatrix} = = \vec{g_1} \vec{g_1}^T c_{11}^{SS} + \vec{g_1} \vec{g_2}^T c_{12}^{SS} + \vec{g_2} \vec{g_1}^T c_{21}^{SS} + \vec{g_2} \vec{g_2}^T c_{22}^{SS}$$
(5)

Or in matrix form:

$$\begin{pmatrix} c_{11}^{MM} & c_{12}^{MM} \\ c_{21}^{MM} & c_{22}^{MM} \end{pmatrix} = \\ = \begin{pmatrix} g_{1}^{1}g_{1}^{1} & g_{1}^{1}g_{1}^{2} \\ g_{1}^{2}g_{1}^{1} & g_{1}^{2}g_{1}^{2} \end{pmatrix} c_{11}^{SS} + \begin{pmatrix} g_{1}^{1}g_{2}^{1} & g_{1}^{1}g_{2}^{2} \\ g_{1}^{2}g_{2}^{1} & g_{1}^{2}g_{2}^{2} \end{pmatrix} c_{12}^{SS} + \\ + \begin{pmatrix} g_{2}^{1}g_{1}^{1} & g_{2}^{1}g_{1}^{2} \\ g_{2}^{2}g_{1}^{1} & g_{2}^{2}g_{1}^{2} \end{pmatrix} c_{21}^{SS} + \begin{pmatrix} g_{2}^{1}g_{2}^{1} & g_{2}^{1}g_{2}^{2} \\ g_{2}^{2}g_{1}^{1} & g_{2}^{2}g_{1}^{2} \end{pmatrix} c_{21}^{SS} + \begin{pmatrix} g_{2}^{1}g_{2}^{1} & g_{2}^{1}g_{2}^{2} \\ g_{2}^{2}g_{1}^{1} & g_{2}^{2}g_{1}^{2} \end{pmatrix} c_{22}^{SS}$$
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Cross-spectrum in detail

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(5)

Signal leakage

ImCoh [Nolte et al., 2004] : drop real part of eq. 5.

Cross-spectrum in detail

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(5)

Signal leakage

ImCoh [Nolte et al., 2004] : drop real part of eq. 5.

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Vectorized equation:

$$\begin{pmatrix} c_{11}^{MM} \\ c_{12}^{MM} \\ c_{22}^{MM} \\ c_{22}^{MM} \\ c_{22}^{MM} \end{pmatrix} = \begin{pmatrix} g_{1}^{1}g_{1}^{1} \\ g_{1}^{1}g_{1}^{2} \\ g_{1}^{2}g_{1}^{1} \\ g_{1}^{2}g_{1}^{2} \\ g_{1}^{2}g_{2}^{2} \\ g_{2}^{2}g_{1}^{2} \\ g_{2}^{2}g_{2}$$

Separating powers and interactions

(6)



Project equation to the orthogonal complement of these vectors

 \mathbf{P} :

$$\begin{split} \mathbf{F} &= [vec(\mathbf{g_1g_1^T}), vec(\mathbf{g_2g_2^T})] \\ \mathbf{F} &= \mathbf{USV^T} \\ \mathbf{U_2} &= [\mathbf{u_1}, \mathbf{u_2}] \\ \mathbf{P} &= \mathbf{I} - \mathbf{U_2U_2^T} \\ \mathbf{C^{\perp}} &= \mathbf{P}vec(\mathbf{C}^{MM}) \end{split}$$

Separating powers and interactions

Finally we get

$$\mathbf{P} \cdot \begin{pmatrix} c_{11}^{MM} \\ c_{12}^{MM} \\ c_{21}^{MM} \\ c_{22}^{MM} \end{pmatrix} (t) = \mathbf{P} \cdot \begin{pmatrix} g_1^1 g_2^1 \\ g_1^1 g_2^2 \\ g_1^2 g_1^2 \\ g_1^2 g_2^2 \\ g_1^2 g_2^2 \end{pmatrix} c_{12}^{SS}(t) + \mathbf{P} \cdot \begin{pmatrix} g_2^1 g_1^1 \\ g_2^1 g_1^2 \\ g_2^2 g_1^1 \\ g_2^2 g_1^2 \\ g_2^2 g_1^2 \end{pmatrix} c_{21}^{SS}(t)$$

We know

$$\mathbf{P}, \begin{pmatrix} c_{11}^{MM} \\ c_{12}^{MM} \\ c_{21}^{MM} \\ c_{22}^{MM} \end{pmatrix} (t), \begin{pmatrix} g_1^1 g_2^1 \\ g_1^1 g_2^2 \\ g_1^2 g_2^1 \\ g_1^2 g_2^1 \end{pmatrix}, \begin{pmatrix} g_2^1 g_1^1 \\ g_2^1 g_1^2 \\ g_2^2 g_1^1 \\ g_2^2 g_1^2 \end{pmatrix}$$

We want to find $c_{12}^{SS}(t), c_{21}^{SS}(t)$

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We need to solve

$$vec(\mathbf{C}^{\perp}(t)) = \sum_{i=1}^{L} \sum_{j=1}^{L} vec(\mathbf{g}_{i}\mathbf{g}_{j}^{\mathbf{T}})^{\perp} c_{ij}^{ss}(t) + vec(\mathbf{C}^{\mathbf{NN}}(t))$$
(7)

 $c_{ij}^{ss}(t)$ are the unknown timeseries on cortex which we are to recover

Global linear problem

PSIICOS objection:

$$vec(\mathbf{C}^{\perp}(t)) = \sum_{i=1}^{L} \sum_{j=1}^{L} vec(\mathbf{g}_{i}\mathbf{g}_{j}^{\mathbf{T}})^{\perp} c_{ij}^{ss}(t) + vec(\mathbf{C}^{\mathbf{NN}}(t))$$
(8)

Define new variables:

Let $\Omega = vec(\mathbf{C}^{\perp}(t))$, $\Gamma_{\mathbf{k}} = vec(\mathbf{g}_{\mathbf{i}}\mathbf{g}_{\mathbf{j}}^{\mathbf{T}})^{\perp}, \sigma_{\mathbf{k}}(t) = c_{ij}^{ss}, \mathbf{N}(t) = \mathbf{C}^{\mathbf{NN}}(t)$; then (8) will look like:

$$\mathbf{\Omega}(t) = \sum_{k=1}^{L^2} \mathbf{\Gamma}_{\mathbf{k}} \sigma_{\mathbf{k}}(t) + \mathbf{N}(t)$$
(9)

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One way to estimate coherent sources is to look at correlation of topographies with signal subspase

$$\begin{split} \boldsymbol{\Omega} &= \mathbf{U}\mathbf{S}\mathbf{V}^{\mathbf{T}}\\ \mathbf{C}_{\mathbf{r}} &= [\mathbf{u}_{1}, \mathbf{u}_{2}, ..., \mathbf{u}_{\mathbf{r}}]\\ A^{(n)} &= \left\{ \boldsymbol{\sigma} \quad \left| \quad \left\| \boldsymbol{\Gamma}_{\sigma}^{\mathbf{T}}\mathbf{C}_{\mathbf{r}} \right\| > threshold \right\} \end{split}$$

Projection effect







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- Three phase-locked networks
- 1/f brain noise
- Networks activity overlap in time
- Induced activity (same frequencies = 10 Hz, different envelopes for each network)
- Bandpass filter 2-20 Hz
- Constant phase shifts $(\pi/20,\pi/2-\pi/20)$ plus random phase
- Solved on grid with 1503 verticies

Source locations:





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Comparison to other algorithms on simulated data



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Precision-recall curves for simulations



Figure: Three networks detection (left: SNR=1, right: SNR=0.2)



Figure: Monte-Carlo networks simulation (left: SNR=1, right: SNR=0.2)

Performance for different phase shifts



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Rotating dipole issue



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Simulations with rotating dipole

Rotation speed: 40 rotations per second. Initial phase is random







PSIICOS (MUSIC scan)













Connectivity measures consistency



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Real data performance example

Band: 8-12 Hz, stimulus: audio odd-ball, trial: 0.4 - 0.7 s







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Real data PSIICOS vs GCS

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300 bootstrap iterations, band: 16-25 Hz



Two different subjects



Band: 16-25, 200 bootstrap iterations

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Monte-Carlo procedure Avarvand et al., IFMBE proceedings, 2010

- 1 Compute ICA on real data
- 2 shift ICA components randomly for each trial
- **3** project back to sensors
- 4 repeat N times
- **5** compute maximum subspace correlation on each iteration
- **6** see, how real data max subspace correlation fits in obtained distribution

Surrogate data results



Real projected vs Imag

Voluntarily finger movement, 3 subjects, real projected cross-spectrum (left) vs imaginary cross-spectrum



200

Thank you!